Hypofractionated and Stereotactic Radiation Therapy

A Practical Guide Orit Kaidar-Person Ronald Chen *Editors*

Second Edition

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A Practical Guide

Second Edition

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Prof. Kaidar-Person would like to dedicate this book in memory of her mentor, Prof. Abraham Kuten, who was a compassionate doctor, mentor, researcher, and family man. A national and international leader in oncology. He will be thoroughly missed.

Prof. Chen would like to dedicate this book to his wife Petronella Muresan, an incredible mother and outstanding statistician; and to their children, Luke Chen and Matthew Chen.

Preface

Radiation therapy (RT) continues to evolve rapidly as a result of improvements in imaging, advances in patient immobilization and treatment delivery technologies, and our understanding of radiobiology. There are currently two major trends in RT, shortening treatment (hypofractionation) and use of stereotactic radiosurgery and stereotactic body radiotherapy technologies. As published data continue to rapidly accumulate, these treatments are no longer exclusive to specialized centers. Shortening treatment is also appealing to patients because of increased convenience, less interference with planned systemic therapy, and is often less costly than conventionally fractionated (longer) RT courses. Radiation therapy continues to be, and is increasingly so, an effective and cost-effective cancer treatment that reduces cancer-specifc mortality (CSM) and overall mortality for many cancers.

This handbook was developed to summarize the data and techniques for hypofractionation and stereotactic radiation in a clinically accessible way, providing concise information ranging from commonly used dose-fractionation schemes to simulation and treatment specifications to published safety and efficacy data. While hypofractionation and stereotactic radiation are used in almost all cancer sites, we note where there are strong supportive data including randomized trials, and other areas where relatively little data are available to guide treatments. Further, we want to highlight that the development of a stereotactic radiotherapy program requires specialized expertise and quality assurance procedures, which are described in Chap. 3.

We hope that you will enjoy the book as much as we enjoyed the process of developing it. This handbook was written to be practical, with usable information relevant for the clinician. We want to thank all the contributors of this book for their hard work and expertise.

Ramat Gan, Israel **Canadian Canadian Canad** Kansas City, KS, USA Ronald Chen

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Chapter 1 The History and Radiobiology of Hypofractionation

Elaine M. Zeman

1.1 Introduction

The use of hypofractionation in radiation therapy is not a new concept. In fact, it is a very old one, dating back to the frst third of the twentieth century, the earliest days of the feld that would evolve into today's specialty of radiation oncology. Since its earliest incarnation, however, hypofractionation has been "repurposed" for today's use, thanks to more than a century of advances in physics and imaging that now allow most normal tissue to be excluded from the radiation feld, something arguably inconceivable in 1900.

To better understand why hypofractionation was largely abandoned by the late 1920s, only to re-emerge at the beginning of the twenty-frst century, an overview of the histories of both radiation therapy and radiation biology is in order. In many ways, these two disciplines evolved in parallel. With a few notable exceptions, for nearly 60 years advances in radiation therapy were empirically based, and advances in radiobiology were seldom of clinical utility. This began to change during the 1950s.

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1.2 Historical Context

1.2.1 The Early History of Fractionation in Radiotherapy

At the turn of the twentieth century, X-rays were discovered by German physicist Wilhelm Röntgen, who described them as invisible, "mysterious" emissions from energized vacuum tubes that were capable of producing fuorescence in platinocyanide salts [1]. The following year, French physicist Henri Becquerel identifed similar emanations from natural substances—compounds of the element uranium—that didn't require an external energy source, yet like visible light, could expose photographic flm [2]. Another year later, Pierre and Marie Curie identifed and isolated some of the elements responsible for this "radioactivity" phenomenon, including radium, thorium, and polonium [3]. That X-rays and radioactive sources (emitting γ-rays) had potential medical applications for both imaging and cancer treatment was immediately obvious, and between 1896 and 1900, the nascent feld of radiation therapy, as practiced by dermatologists and surgeons of the day, had already claimed cures of both benign and malignant skin conditions [4–6].

In the earliest days of radiotherapy, both X-ray machines and radium applicators were used for cancer treatment, although the greater availability, convenience, and portability of X-ray tubes afforded them a distinct advantage. Add to this the fact that X-ray machines offered*,* as the technology improved, much higher intensities of radiation output than low-activity radium sources, radiotherapy using X-rays (termed teletherapy) quickly became the international standard. Nevertheless, the use of radioactive sources continued to be developed and refned by the French, a practice that evolved into modern day brachytherapy.

Lacking an understanding at the time of the physical nature of ionizing radiation and how to quantify radiation dose, let alone an understanding of its biological effects, various "philosophies" developed as how best to treat patients. One fundamental radiotherapy principle was recognized early on: the concept of the therapeutic ratio, a risk-versus-beneft approach applied to treatment planning (Fig. 1.1).

In theory, any malignancy could be eradicated simply by delivering a sufficiently high radiation dose. However, in practice, injury to normal tissues that were necessarily irradiated along with the tumor limited the total dose that could be administered safely. Therefore, a balance had to be struck between what was considered an acceptable probability of radiation-induced damage to normal tissue, and the probability of tumor destruction.

Because surgeons were among the early practitioners of radiation therapy, from about 1900 into the 1920s, a prevailing strategy was to view radiotherapy as akin to surgery; that is, to attempt to eradicate the tumor in a single procedure using a large, "tumoricidal" dose. This massive dose technique [7, 8] became a common way of administering radiation therapy, and a (somewhat arbitrary) biological interpretation was also provided: tumors would become increasingly resistant to radiotherapy if too many doses were given, and normal tissues would be preferentially damaged due to "cumulative injury," so it would be preferable to deliver the radiation therapy

Fig. 1.1 The therapeutic ratio concept, depicted graphically. A favorable therapeutic ratio implies that the radiation response of the tumor is greater than that of the surrounding normal tissue (left panel). In the case of an unfavorable therapeutic ratio (right panel), there is no possibility of obtaining good tumor control without signifcantly damaging the normal tissue(s) at risk. (Adapted from Bernier et al. [7])

as one or a few large doses over no more than a few days [9]. However, it soon became obvious that this approach did not optimize the therapeutic ratio and that the biological rationale was incorrect; normal tissue complications were typically quite severe, and to make matters worse, the rate of local tumor recurrence was unacceptably high. An early example, in this case involving treatment of a benign hairy nevus, is shown in Fig. 1.2.

As mentioned previously, radium therapy was used more extensively in France. Radium applications involved longer overall treatment times in order to reach total doses comparable to those achieved with X-rays because of the low activity sources. Although multi-day treatments were less convenient in terms of patient throughput, clinical outcomes were often superior for skin and cervix cancers than for X-ray therapy. Brachytherapy proponents also offered a biological rationale, one that was better based on laboratory research than on theory or conjecture. As early as 1906, two French radiation biologists, Bergonié and Tribondeau, observed histologically that undifferentiated, rapidly dividing spermatogonia of the rat testis showed evidence of damage at lower radiation doses than well-differentiated, non-dividing cells of the testicular stroma. Based on these observations, they put forth some basic "laws" stating that radiotherapy was selective for cells that were (1) actively dividing; (2) capable of dividing for extended periods; and (3) poorly or undifferentiated

Fig. 1.2 Time course for radiation effects in the skin of a child treated during the "massive dose" era for an extensive hairy nevus before treatment (left), a week after the end of treatment (middle) and 75 years later (right). Acutely, the skin injury consisted of a large area of confuent moist desquamation, but over time, fbrosis, necrosis, and poor wound healing was observed and persisted over the patient's lifetime. Few patients were cured using this large dose, large volume technique, and typically died long before normal tissue damage became manifest. In this particular case, however, the (benign) hairy nevus was eradicated. (Adapted from Kogelnik [5])

[10]. Some tumors were already known at that time to contain cells that were less differentiated and more proliferative than most normal tissues. Accordingly, Bergonié and Tribondeau reasoned that multiple radiation exposures would preferentially kill these tumor cells, while preserving their slowly proliferating, differentiated counterparts in the normal tissues included in the radiation feld.

During the 1920s, the massive dose technique began to fall out of favor, particularly in light of the pioneering experiments of Claude Regaud and colleagues, who built on Bergonié and Tribondeau's earlier work [11]. Regaud cleverly used the testes of the rabbit as a model system, reasoning that the process of sperm production (i.e., relatively undifferentiated cells proliferating rapidly and indefnitely) mimicked to a frst approximation the behavior of tumors, and that the scrotum could be used as a representative dose-limiting normal tissue. Regaud showed that only through the use of multiple, smaller radiation doses could animals be completely sterilized without producing severe injury to the scrotum [12].

These principles were soon tested in the clinic by French physician Henri Coutard, who used multiple small x-ray doses delivered over extended periods in human patients [13]. Clinical outcomes for patients with head and neck cancer were improved to such an extent that fractionated radiation therapy using many small dose increments spread over several weeks' time soon became the standard of care [13, 14], and has largely remained so to the present day.

Summary: relevance to today's use of hypofractionation

- During the early days of radiotherapy—the frst 30 years of the twentieth century—extreme hypofractionation using one or a few very large doses was a treatment standard.
- It was subsequently abandoned when it became clear that tumor control was poor and normal tissue complications severe.
- Early research in radiation biology determined that the best way to optimize the therapeutic ratio was to deliver many small dose fractions over a period of weeks.
- Translating this information into the clinic, fractionated radiotherapy using small doses delivered over several weeks provided much improved outcomes, and became the new standard of care.

1.2.2 Isoeffect Relationships

Once fractionated radiotherapy became the new standard of care a different problem emerged, namely how different practitioners with somewhat different approaches to fractionation, e.g., how many fractions delivered, time between fractions, total dose, overall treatment time, etc., could be inter-compared in terms of tumor control and normal tissue complication probabilities. One approach was to determine "equivalents," that is, treatment combinations that yielded similar outcomes. Time-dose equivalents for skin erythema were published by several investigators [15–18] and these formed the basis for the calculation of equivalents for other normal tissue and tumor responses. By plotting the total dose required for a particular equivalent in a particular tissue, as a function of one of the variable treatment parameters (overall treatment time, number of fractions or dose per fraction), a so-called isoeffect curve could be derived. All time and dose combinations that comprised an isoeffect curve for a certain endpoint would, theoretically, produce tissue or tumor responses of equal magnitude.

Also better appreciated during the 1930s was how and when normal tissue complications occurred after treatment, and their severity as a function of total dose. Presumably, these complications were the result (directly or indirectly) of the killing of critical cells within the tissue, so the higher the radiation dose, the more cells were killed and the more severe the complication. It was also clear that skin, the dose-limiting normal tissue in most cases, could manifest more than one complication and that each seemed to have its own threshold or tolerance dose before the complication occurred, a refection of the tissue's radiosensitivity. However, the "earliness" or "lateness" of the clinical manifestation of that injury was a separate phenomenon more related to the cellular renewal pattern of the tissue.

The frst published isoeffect curves were produced by Strandqvist in 1944 [19], and shown in Fig. 1.3. When plotted on a log–log scale of total dose versus overall treatment time, isoeffect curves for a variety of skin reactions, and the cure of skin cancer, were drawn as parallel lines.

As drawn, Stranqvist's isoeffect curves suggested that there would be *no* therapeutic advantage to using prolonged treatment times and multiple small dose

Fig. 1.3 Strandqvist's isoeffect curves, frst published in 1944, plotted the log of the total dose to achieve the measured isoeffect as a function of the overall treatment time. The shorter the overall treatment time, the more hypofractionated the schedule, and the lower the dose required to produce the isoeffect. (Modifed from Strandqvist [19])

fractions for the preferential eradication of tumors while staying within the tolerance of the normal tissue [20]. Ironically however, it was already known that the therapeutic ratio *did* increase with prolonged, as opposed to very short, overall treatment times. Nevertheless, the reliability of these curves at predicting skin reactions, which were the dose limiting at the time, made them quite popular.

Nearly 25 years after Strandqvist, Ellis [21, 22] revisited his popular isoeffect curves, and armed with new knowledge about the radiobiology underlying fractionation effects in pig skin [23, 24], formulated the NSD concept in 1969. The NSD equation,

$$
D = (NSD) N^{0.24} T^{0.11},
$$

where *D* is the total dose delivered, *N* the number of fractions used, *T* the overall treatment time, and NSD the nominal standard dose (a proportionality constant related to the tissue's tolerance), became widely used, particularly once mathematically simplifed derivatives, such as the TDF equation [25] became available. The major innovation of the NSD model was that the infuence of the fraction number had been separated from the infuence of the overall treatment time, and in fact, the fraction number (and therefore, size) was the more important of the two.

The introduction of the NSD equation allowed radiotherapy treatment practices world-wide to be compared with respect to putative "biological equivalence," provided it was not used for treatments involving extremes of fraction number or overall time outside the range of the data upon which the model was based (i.e., Strandqvist's curves). It also provided a means of revising treatment prescriptions in the event of unforeseen treatment interruptions. However, the NSD formula was illequipped to deal with some clinical issues, in particular the prediction of late effects in normal tissues, which, with the advent of megavoltage linear accelerators capable of treating deep-seated tumors, replaced skin as being dose-limiting [26]. In light of the emerging limitations of the NSD model, there was a need for new, radiobiologically based approaches to isoeffect modeling.

Summary: relevance to today's use of hypofractionation

- Isoeffect curves plot the total dose required for a particular tumor or normal tissue endpoint as a function of one of the variable treatment parameters, such as overall treatment time or number of fractions. All time-dose combinations that fell on a particular isoeffect curve were considered biologically equivalent.
- Isoeffects of interest included tumor control and various normal tissue complications, typically in skin, such as desquamation, necrosis, or fbrosis.
- Some complications occurred during or soon after the completion of radiotherapy, "early effects," and others took months or years to manifest, "late effects."
- The total dose required to cause a particular complication was a refection of the tissue's radiosensitivity, but the time it took for the complication to appear was related to the tissue's natural cell renewal process.
- A mathematical model derived from isoeffect curves, the NSD equation, allowed the calculation of biological equivalents for different treatment schedules. Yet because the model was based on early skin reactions, it was poorly equipped to model late complications in normal tissues. With the advent of megavoltage radiotherapy equipment that allowed treatment of deep-seated tumors, damage to internal organs rather than skin became dose-limiting, and many of these expressed their injuries as late effects.

1.2.3 Tumor Hypoxia

As early as 1909, it was recognized that decreasing blood fow during radiotherapy leads to a reduction in the prevalence or severity of radiation-induced skin reactions [7, 8], although at the time, the mechanism for this effect was unclear. Decades later, chemists and biologists determined that the presence or absence of oxygen was the key, and that the mechanism of oxygen's action was to interact with free radicals produced during irradiation, thereby enhancing the damage to cellular macromolecules. In other words, oxygen acted as a radiation sensitizer. Thus, the relative *absence* of oxygen in an irradiated system meant less molecular damage, and therefore, greater radioresistance.

In 1955, however, Thomlinson and Gray [27] brought this idea to the forefront of radiation biology and radiation therapy by proposing that tumors contained a fraction of oxygen-starved yet still reproductively viable (i.e., "clonogenic") hypoxic cells and that if these persisted throughout the course of fractionated radiotherapy, they would adversely affect the therapeutic ratio. The oxygen enhancement ratio (OER) is a metric developed to quantify how much more radioresistant hypoxic cells were than well-aerated ones. For large, single radiation doses, OER values of 2.5–3.0 were typical, but for conventional radiotherapy using repeated, small dose fractions delivered over several weeks, the OER was lower, typically in the range of $1.5 - 2.0$ [28].

Accordingly, if human tumors contained even a tiny fraction of clonogenic hypoxic cells, simple calculations suggested that tumor control would be nearly impossible [29], even for high doses. The total dose needed to control such tumors would become prohibitive because normal tissues are not hypoxic and therefore would experience higher complication rates if the total dose were increased. In fact, the only way that hypoxic tumor cells would *not* constitute a treatment impediment was if extended periods of hypoxia eventually led to their deaths, that these cells "reoxygenated" during the course of treatment and/or that they were not clonogenic to begin with.

Hypoxia is a consequence of the abnormal vasculature characteristic of tumors. Such blood vessels are the product of abnormal angiogenesis and often are structurally, functionally, physiologically, and/or spatially aberrant which, when combined with the tumor's high oxygen demand and tendency to outgrow its own blood supply, leads to both micro- and macro-regions of hypoxia.

Summary: relevance to today's use of hypofractionation

- Molecular oxygen interacts with free radicals produced during irradiation, enhancing cellular damage. Hypoxic cells that are low in oxygen, but not so low as to result in lethality, can be up to three times more radioresistant than wellaerated ones.
- Vascular abnormalities characteristic of tumors lead to both micro- and macroregions of hypoxia. Hypoxia is largely absent in normal tissues.
- Simple calculations suggest that tumor control would be impossible—even for the high doses used today in extreme hypofractionation—if human tumors contained even a tiny fraction of clonogenic hypoxic cells, provided they persisted throughout the course of radiotherapy.

1.2.4 The Four R's of Radiotherapy

What was largely lacking during radiotherapy's frst half-century was a biological basis for why dose fractionation spared normal tissue complications, and without this information, it was very diffcult to determine which biological characteristics of normal or tumor tissues might be exploited to improve the therapeutic ratio. This began to change with the publication in 1975 of a seminal paper entitled "*The Four R's of Radiotherapy*" [30]. The paper was an attempt to explain the biological basis of fractionation by describing in simple terms key radiobiological phenomena thought to affect radiotherapy outcome: *R*epair, *R*epopulation, *R*eoxygenation, and *R*edistribution. In the ensuing years, a ffth "R" was added, *R*adiosensitivity [31], although in some respects, it is inextricably linked to repair. (Redistribution is difficult to measure, yet is assumed to occur in vivo during conventional fractionation. However, it is thought to play only a minor role in treatment outcome and likely has even less of a role for hypofractionation, so will not be discussed further.)

1.2.4.1 Repair and Radiosensitivity

The surviving fraction of cells following a moderate-to-high radiation dose is higher if that dose is split into two increments separated by a time interval than delivered as a single dose, suggesting that cells surviving the initial dose had repaired some of the damage during the radiation-free interval [32]. As such, this damage was no longer available to interact with the damage inficted by the second dose, so a higher cell surviving fraction resulted. This phenomenon is termed sublethal damage recovery (SLDR). These "split-dose" experiments turned out to be crucial to the understanding of why and how fractionated radiation therapy works, that is, that SLDR was responsible for the greater radiation tolerance of tissues when a large total dose was divided into small dose fractions and protracted over time.

However, this sparing effect of dose fractionation does not continue indefnitely as smaller and smaller (and more numerous) doses are delivered. Instead, a limit is reached where further lowering of the dose per fraction does not produce a further decrease in toxicity. This fnding is consistent with the idea that survival and dose response curves have negative initial slopes [33, 34], and that after many, sufficiently small dose fractions are delivered, a "trace" of this initial slope would be obtained.

One important clinical implication of repair and radiosensitivity phenomena is that small differences in shoulder regions of dose response curves for different doselimiting normal tissues and tumors could be magnifed into large differences when many small dose fractions are used compared to a single or a few large fractions. A tissue's radiosensitivity and repair capacity are critically important to the selection of the total dose, dose per fraction and interfraction interval used for radiation therapy, as they govern both the tumor control and normal tissue complication probabilities.

1.2.4.2 Repopulation

Repopulation is defned as an increase in cell proliferation in tissues in response to an injury that produces cell killing. Normal tissues and tumors containing stem or stem-like cells can begin to proliferate during and after a course of radiation therapy, with the timing of this response a function of the proliferation kinetics of the tissue [35, 36], typically during or within 3 months of treatment for "earlyresponding" normal tissues and most tumors, and more than 6–9 months (if at all) for "late-responding" tissues.

Repopulation is desirable in normal tissues because it facilitates the healing of common radiotherapy complications that develop during or soon after treatment, such as oral mucositis, for example. On the other hand, repopulation of tumor cells is undesirable because it would have the net effect of counteracting ongoing radiation therapy, which in turn would lead to the appearance of tumor "radioresistance" and accordingly, the attendant risk of recurrence. For tumors capable of rapid repopulation that begins during conventional radiotherapy, estimates are that as much as